

Pharmacokinetic Profile of Dodecanedioic Acid, a Proposed Alternative Fuel Substrate

G. MINGRONE,* A. V. GRECO,* A. DE GAETANO,† A. TATARANNI,* C. RAGUSO,* AND M. CASTAGNETO†

From the *Istituto di Clinica Medica and †Istituto di Clinica Chirurgica, Centro per lo Studio della Fisiopatologia dello Shock, Università Cattolica S. Cuore, Roma

ABSTRACT. Dodecanedioic acid (C12), a saturated, aliphatic dicarboxylic acid with 12 carbon atoms, was given as an intravenous bolus (800 $\mu\text{mol/kg}$ of body weight [kg_{BW}]) in male Wistar rats to study its pharmacokinetic profile. Because total plasma C12, which results from the sum of both free and albumin binding fractions, was measured by high-performance liquid chromatography, an *in vitro* experimental session was carried out to determine the binding curve of C12 in rat plasma. These data were then used to calculate the plasma C12 free fraction in *in vivo* experiments. The best fit obtained for the experimental data of albumin binding was obtained with the equation of reversible, saturable binding to one, two, or three classes of noninteracting equivalent sites. Only a single binding site was clearly identified with a dissociation constant of 147 $\mu\text{mol/L}$ and a maximal predicted binding of 1.57 mol/mol

albumin. The urinary excretion of C12 was $3.90 \pm 1.62\%$ of the administered dose. The pharmacokinetic analysis was performed by one-compartment model with linear transfer to the tissues, taking into account simultaneously both plasma concentration and urine excretion data. The apparent volume of distribution of C12 was $0.248 \pm 0.035 \text{ L/kg}_{\text{BW}}$, the apparent first order rate constant to the tissues was $0.0535 \pm 0.0123 \text{ min}^{-1}$ and that from plasma to urine was $0.00206 \pm 0.00051 \text{ min}^{-1}$. The C12 plasma half-life was 12.47 minutes. Renal clearance was $0.00051 \text{ L/kg}_{\text{BW}}$ per minute, whereas the systemic clearance was $0.0138 \text{ L/kg}_{\text{BW}}$ per minute. Because the renal clearance was much less than the rat inulin clearance reported in literature, the presence of C12 passive back-diffusion was hypothesized. (*Journal of Parenteral and Enteral Nutrition* 18:225-230, 1994)

The use of the salts of dicarboxylic acids (DAs) as a possible fuel substrate in parenteral nutrition¹⁻⁶ was recently proposed. The theoretical basis of this contention is that salts of DAs (1) are highly water soluble and, compared with both long-chain and medium-chain fatty acids, are bound less avidly by albumin⁷⁻⁹; (2) undergo β -oxidation at the level of both mitochondria and peroxisomes at a high rate¹⁰⁻¹⁴; (3) do not induce ketogenesis^{5,15} as medium-chain triglycerides do,^{16,17} but rather promote gluconeogenesis via succinate production during their β -oxidation¹⁸; (4) do not require hydrolysis before tissue uptake and therefore could represent an immediately available form of energy; and (5) can be easily and inexpensively prepared because they are water soluble.

In spite of these theoretical advantages over the usual lipid substrates (long-chain and medium-chain triglycerides), the DAs studied for nutritional purposes have been subject to high urinary excretion until now. Depending on the administered dose, 50% to 70% of azelate (C9) and 16% to 46% of sebacate (C10) are eliminated in the urine.^{1-6,19}

Therefore, the aim of this study was to investigate the nutritional potential of the 12-carbon DA, C12, in the laboratory animal with special reference to its pharmacokinetic profile and urinary excretion characteristics, in view of its possible use as a fuel substrate in humans.

MATERIALS AND METHODS

Equilibrium Dialysis

Binding of C12 to rat serum albumin was determined by using equilibrium dialysis. Dialysis apparatus (Spectra/Por Equilibrium Dialyzer) and membranes were from Spectrum (Houston, TX). The chamber contains two 1-mL compartments separated by a dialysis membrane that is permeable to compounds with a molecular weight < 6000; albumin does not cross the dialysis membrane.²⁰ Preliminary experiments showed that C12 reaches equilibrium within 3 hours at 37°C and 25 rpm. Thus, we chose a 4-hour incubation period to ensure equilibrium. Binding was assessed by adding varying concentrations of C12 (100 to 6000 $\mu\text{mol/L}$) to samples of DA-free rat plasma. Plasma with added C12 was placed in one side (side A) of the chamber and a salt solution containing 0.116 mol/L sodium chloride, 0.0049 mol/L potassium chloride, and 0.016 mol/L sodium phosphate at pH 7.4 was added to the other side (side B). Dialysis chambers were put into a constant-temperature (37°C) water bath and were rotated at 25 rpm. At

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Correspondence and reprint requests: G. Mingrone, MD, Istituto di Clinica Medica, Università Cattolica S. Cuore, Largo A. Gemelli, 8, 00168 Roma, Italy.

the end of the incubation period, 0.5 mL was removed from each side and the concentration of C12 was measured by high-performance liquid chromatography as previously described.³ Azelaic acid (50 µg) was used as an internal standard. The concentration of bound C12 was determined by subtracting the concentration of C12 found in side B from the concentration of C12 in side A. This was then normalized for the measured albumin concentration and to the volume of the dialysis chamber.

In Vivo Experiments

Male Wistar rats weighing between 170 and 250 g were used in all the experiments. The rats were injected intravenously (intravenous tail vein injection) with 800 µmol of C12 per kilogram of body weight (kg_{BW}) in the form of disodium salt as a bolus. Blood samples were drawn by cardiac puncture, then the animals were killed by cervical dislocation. Heparinized blood samples were immediately centrifuged at $4000 \times g$ and plasma was frozen at $-20^\circ C$ until analysis.

Five rats, treated as described above, were allocated to individual metabolic cages for the collection of 24-hour urine. DAs in both plasma and urine were measured by high-performance liquid chromatography as previously described.³

Albumin Binding Model

Dodecanedioic binding in plasma was assessed by a one-site model (Table I) according to the methods of Tonsgard and Meredith.⁷ The model was fitted by unweighted nonlinear least squares, using the inverse Hessian method to derive the estimates of the parameter dispersions. A two-site model was not shown to be superior to the one-site model for explaining the binding curve. A stoichiometric approach was also followed: the two-step stoichiometric model was equivalent to the one-site model, and the one-site model was chosen for comparability with previously published results.^{7,8} A three-step stoichiometric model was no better than the two-step model.

Pharmacokinetic Analysis

Two basic models were compared (Tables II and III); both were one-compartment models with linear transfer to the tissues, taking into account simultaneously both plasma concentration and urine excretion data. In model

TABLE I
Dodecanedioic acid binding model

$$r = S_B f / (K_B + f) \quad r = b/a$$

where

f = free dodecanedioic acid ($\mu\text{mol/L}$);

b = bound dodecanedioic acid ($\mu\text{mol/L}$);

a = serum albumin concentration ($\mu\text{mol/L}$);

S_B = predicted saturation (mol C12/mol albumin); and

K_B = dissociation constant ($\mu\text{mol/L}$)

Fitted parameters

$$S_B = 1.57 \pm 0.05 \text{ mol C12/mol albumin}$$

$$K_B = 147 \pm 23 \mu\text{mol/L}$$

A, a simple linear renal excretion mechanism was presumed, represented by the apparent first-order rate constant k_{12} . In model B, a nonlinear renal excretion mechanism was allowed for, which resulted from the sum of a linear component ($k_{12} C_{1F}$) and a saturable transport [$T_{12} C_{1F} / (M_{12} + C_{1F})$]. Both models were fitted by nonlinear least squares with a quasi-Newton algorithm. Estimates of the parameter dispersions were obtained from the diagonal elements of the inverse Hessian at the minimum.

RESULTS

The binding of monocarboxylic fatty acids to albumin modulates their transport to tissues and their cellular uptake.^{21,22} Therefore, we have assumed albumin to be or to closely represent the principal species of DA carrier in plasma. Data are reported in the literature about C12 binding to defatted serum bovine albumin.^{7,8} Such data, which are of great interest in elucidating the structure of the albumin binding sites for DAs, are of limited value in quantifying the real amount of DA bound in plasma, because many less-water-soluble compounds are normally present in plasma and compete for transport. Therefore, we chose to directly determine the binding curve of C12 in normal plasma by equilibrium dialysis.

Figure 1 shows the best fit obtained for the experimental data by using a one-site model. Only a single binding site for C12 can be clearly identified with a dissociation constant of $147 \pm 23 \mu\text{mol/L}$ (coefficient of variation = 15.6%) and a maximal predicted binding of $1.57 \pm 0.05 \text{ mol/mol albumin}$ (coefficient of variation = 3.5%, $R^2 = 79\%$). The mean \pm SEM 24-hour urinary

TABLE II
One-compartment linear excretion bolus model with urinary data
(model A)

$$c_{1T}(0) = D / (V_1 W)$$

$$dc_{1T}/dt = -(k_{12} c_{1F}) - (k_{10} c_{1T})$$

$$q_2(0) = 0$$

$$dq_2/dt = k_{12} c_{1F} V_1 W$$

$$c_{1F} = 0.5 [c_{1T} - C_{BS} - K_B + (C_{1T} - C_{BS} - K_B)^2 + 4 K_B c_{1T}] \div 2$$

where

V_1 (L/ kg_{BW}) is the apparent volume of distribution;

c_{1T} and c_{1F} ($\mu\text{mol/L}$) are total and free plasma C12 concentrations, respectively

q_2 (μmol) is the amount of C12 loss with urine;

D (μmol) is the intravenously administered dose;

W (kg) is the body weight;

k_{10} (fraction/min) is the apparent first-order rate constant from plasma to tissues;

k_{12} (fraction/min) is the apparent first-order constant from plasma to urine;

C_{BS} ($\mu\text{mol/L}$) is the bound C12 at saturation = $1.57 \times$ albumin ($\mu\text{mol/L}$); and

K_B ($\mu\text{mol/L}$) is the dissociation constant = 147

Fitted parameters

$$V_1 = 0.248 \pm 0.035 \text{ L/kg}_{BW}$$

$$k_{10} = 0.0535 \pm 0.0123 \text{ min}^{-1}$$

$$k_{12} = 0.00206 \pm 0.00051 \text{ min}^{-1}$$

kg_{BW} , kilogram of body weight.

excretion of C12 was $3.901 \pm 1.62\%$ of the administered dose.

Although the fit of model A to the data was good ($R^2 = 69\%$) and parameter estimates were stable with narrow confidence limits, the fitting of the nonlinear model B was good but gave rise to very unstable estimates of parameters k_{12} , T_{12} , and M_{12} . Inasmuch as the urinary excretion of the compound is very small, the random scatter of the data points was greater than the quantifiable effect of a possible saturable transport mechanism. The T_{12} found ought to be regarded as uninformative, especially taking into account its very large standard error. For this reason, model A was chosen as being the most conceivable representation of DA disposition.

Figure 2 depicts the concentration profiles (predicted by the model by using the estimated values of the pharmacokinetic parameters) together with all the individual experimental data on plasma concentration. The apparent volume of distribution of C12 was 0.248 ± 0.035 L/kg_{BW}. The apparent first-order rate constant to the tissues (k_{10}) was 0.0535 ± 0.0123 min⁻¹, whereas that from plasma to urine (k_{12}) was 0.00206 ± 0.00051 min⁻¹. The C12 plasma half-life was 12.47 minutes. Renal clearance was 0.00051 L/kg_{BW} per minute, whereas systemic clearance was 0.0138 L/kg_{BW} per minute. Therefore, renal clearance is much less than the reported inulin clearance in the rat (0.0101 ± 0.0004 L/kg_{BW} per minute),²³ suggesting the presence of a C12 passive back-diffusion or an active reabsorption from the renal tubules to plasma.

DISCUSSION

Some years ago in a very interesting and original publication titled "Dicarboxylic Acids and the Lipid Metabolism," Mortensen stressed the concept of nonketotic dicarboxylic aciduria.²⁴ This term was used to indicate the presence of DA in the urine of subjects affected by congenital or acquired defects of fatty acid β -oxidation. Glutaric aciduria type II²⁵⁻²⁹ is one congenital disease that causes dicarboxylic aciduria. Other similar

congenital defects have been described in patients who died on the day of birth because of lactate acidosis³⁰⁻³³ or survived the neonatal period but subsequently suffered a number of hypoglycemic attacks with simultaneous increases in DA excretion. All these patients showed a genetic defect of fat oxidation localized to the medium-chain acyl-CoA dehydrogenase. The authors³⁰⁻³³ hypothesized that the DAs were formed from an ω -oxidation of medium-chain monocarboxylic acids that had accumulated because of the metabolic blockade.

Reye's syndrome was first described as a distinct clinical and pathologic entity in 1963.³⁴ This syndrome is characterized by encephalopathy and cellular fatty degeneration. The presence of a viral-type prodrome led investigators^{35,36} to suspect viruses as causative agents. Histochemical analysis of mitochondrial enzymes in liver tissue from patients with Reye's syndrome showed that the activities of both succinic acid dehydrogenase and cytochrome oxidase were depressed in the presence of nicotinamide adenine dinucleotide-tetrazolium reductase and ubiquinone, suggesting an injury to either the tricarboxylic acid cycle or the electron transport system.³⁷ In these patients, the ingestion of toxins such as aflatoxins³⁸ and pesticides³⁹ or of some medications such as salicylates⁴⁰ may precipitate general conditions, acting as contributory causative agents. In a study on the causative role of DAs in Reye's syndrome, Tonsgard and Getz⁴¹ showed that, when C10 was added to normal serum to obtain concentrations of 0.4 mmol/L and mitochondria were incubated in this medium, a reduction in adenosine triphosphate formation was observed (from 454 to 368 nmol) and the respiration was stimulated (77% compared with 33% in the presence of normal serum alone). However, the uncoupling effect of oleic acid at the same concentration was 173%.⁴¹ Previously, Passi et al⁴² hypothesized that there is a toxic effect of medium-chain-length DAs on mitochondrial respiration. This hypothesis was based on the observation that, in the presence of C8-C13 DAs, respiration was inhibited and the degree of inhibition correlated with the chain length of the diacids up to C12. However, this effect

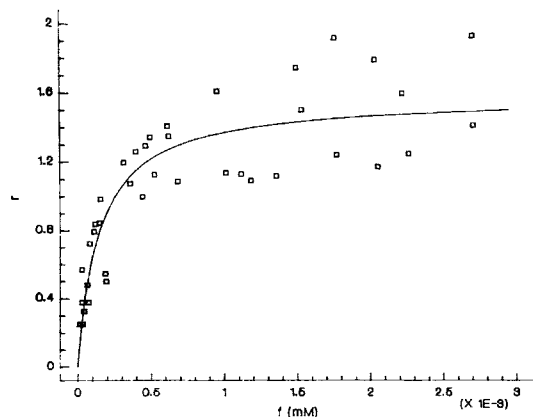


FIG. 1. Binding of disodic dodecanedioate to rat plasma proteins. Because albumin quantitatively represents the most important plasma protein fraction, the values of bound C12 are normalized for the concentration of plasma albumin. r is the molar ratio (mmol/mmol) between bound C12 and plasma albumin. The points ($n = 49$) are experimental data and the line is the best fit of the data to the theoretical equation.

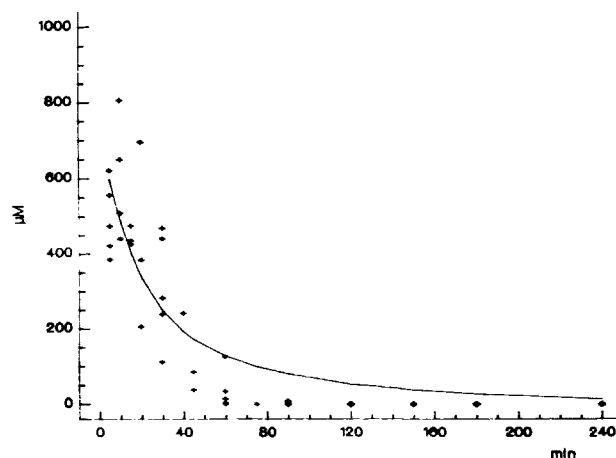


FIG. 2. Plasma concentrations of free C12 ($\mu\text{M/L}$) vs time (minutes) after administration of 800 $\mu\text{mol/kgBW}$ of C12 as an intravenous bolus. Experimental data are fitted by nonlinear least squares with a quasi-Newton algorithm.

was obtained at DA concentrations in the medium on the order of 0.1 to 0.2 mol/L, which correspond, in the case of C12, to levels as high as 2.3 mg/mL. It is also necessary to point out that these elevated concentrations of C12 should be attained in the cell where the mitochondria are located. In addition, Passi et al⁴² found that this inhibition was partially reversible after 1 hour of incubation. Moreover, the same group of researchers⁴³ stated that "C9 to C12 dicarboxylic acids do not have toxic effects on normal cells *in vivo*."

Among the acquired conditions of dicarboxylic aciduria are hypoglycine A intoxication and valproate treatment. Jamaican vomiting sickness⁴⁴ occurs after intake of unripe akee fruit. The fruit's content of hypoglycine A, acting through its metabolite, methylenecyclopropyl acetic acid, inhibits fatty acid oxidation and precipitates acute symptoms similar to those of Reye's syndrome. Mortensen et al⁴⁵ proposed that valproate, an unphysiologic monocarboxylic acid (2-propylpentanoic acid), also acts by inhibiting the oxidation of fatty acids. Therefore, in those pathologic conditions in which a partial or total block of fatty acid mitochondrial β -oxidation is present, dicarboxylic aciduria takes place. DA production represents a protective mechanism for the organism, inasmuch as it is well known that long-chain monocarboxylic acids, particularly if unsaturated, are highly toxic for mitochondria because of their uncoupling effect.^{46,47} When free fatty acid β -oxidation is impaired, free fatty acids are ω -oxidized to long-chain DAs, which can then be β -oxidized at the level of peroxisomes and partially excreted with urine because they, unlike long-chain monocarboxylic acids, are relatively water soluble: their water solubility decreases with chain length. In addition, there is experimental evidence⁴⁸⁻⁵¹ that the ω -oxidation of even-chain monocarboxylic fatty acids makes it possible to convert them into metabolites with a gluconeogenic potential, whereby the oxidation of the synthesized DAs would result in a net production of the citric cycle intermediary, succinyl-CoA.

TABLE III
One-compartment linear + saturable excretion bolus model
with urinary data (model B)

$$c_{1T}(0) = D/(V_1 W)$$

$$dc_1/dt = -(T_{12} c_{1F})/(M_{12} + c_{1F}) - k_{12} c_{1F} - k_{10} c_{1F}$$

$$q_2(0) = 0$$

$$dq_2/dt = [(T_{12} c_{1F})/(M_{12} + c_{1F}) + k_{12} c_{1F}] V_1 W$$

where quantities have the same meaning as in Table II and

T_{12} ($\mu\text{mol}/\text{min}$) = maximal transport (positive = secretion; negative = reabsorption)

M_{12} ($\mu\text{mol}/\text{L}$) = concentration of half-maximal transport

Fitted parameters

$$V_1 = 0.221 \pm 0.065 \text{ (L/kg}_{\text{BW}}) \text{ (CV} = 29\%)$$

$$k_{10} = 0.0438 \pm 0.0166 \text{ (min}^{-1}) \text{ (CV} = 38\%)$$

$$T_{12} = 2.93 \pm 37.3 \text{ (}\mu\text{mol}/\text{min}) \text{ (CV} = 1270\%)$$

$$M_{12} = 980 \pm 1176 \text{ (}\mu\text{mol}) \text{ (CV} = 120\%)$$

$$k_{12} = 0.000117 \pm 0.0199 \text{ (min}^{-1}) \text{ (CV} = 17,000\%)$$

kg_{BW}, kilogram of body weight; CV, coefficient of variation.

In the light of previous studies on shorter-chain-length DAs, ie, azelaic and sebacic acids,^{1,6} C12 appears to be a possible fuel substrate in parenteral nutrition, at least from a theoretical point of view. In the present paper, we have studied the pharmacokinetics of C12 in rats after intravenous bolus administration; an investigation of C12's *in vitro* binding kinetics was also performed to evaluate its affinity to rat albumin.

No data are reported in the literature concerning dodecanedioic renal elimination. In their papers, Ullrich et al^{52,53} localized the transport systems for DAs with a chain length equal to or shorter than 10 carbon atoms at the level of the proximal renal tubule of rat kidney. Our data indicate that the renal elimination of C12 is mainly a linear phenomenon. It results from the glomerular filtration of the compound and from its possible passive back-diffusion along the concentration gradient created by tubular water reabsorption. A carrier-mediated, saturable transport mechanism by the tubules could also exist, but if this is the case, it is not likely to be of any major importance either in the excretion or active reabsorption of the compound.

Tonsgard et al⁷ determined the parameters for binding of C12 (as well as other DAs) on defatted serum bovine albumin. Performing a new binding experiment of C12 on plasma was deemed necessary to quantify the actual amount of binding in actual physiologic conditions. However, the results we obtained are very close to those reported by Tonsgard et al.⁷ In particular, the C12 binding affinity in rat plasma (147 $\mu\text{mol}/\text{L}$) is intermediate between that obtained by Tonsgard et al⁷ without (75 $\mu\text{mol}/\text{L}$) and with (339 and 707 $\mu\text{mol}/\text{L}$) oleic acid at different concentrations. We therefore conclude that albumin binding of C12 is little affected by competitors normally present in plasma.

The loss of C12 in the urine is very small compared with that of other shorter-chain DAs (ie, azelaic and sebacic acids). Azelaic acid, in fact, showed a very high urinary excretion varying from 50%¹ to 76.9%¹⁹ depending on the dose administered and the infusion rate. Sebacic acid was excreted in the urine to a lesser extent, varying from 16%⁴ to 46%⁵ of the given dose, again depending on the amount of sebacate infused, the infusion rate, and—as for azelaic acid—the interindividual variability, which appears to be considerable.

As already pointed out, DA β -oxidation can take place in both peroxisomes and mitochondria.^{10,11} However, *in vitro* oxidation of medium-chain DAs of various lengths (including C12) by isolated hepatocytes seems to take place mainly in the peroxisomes.¹¹ On the other hand, Draye et al⁵⁴ in whole-animal studies showed that C12 is mainly a mitochondrial substrate. The high global oxidation of C12 observed by these authors in laboratory animals can probably be explained by the predominance of skeletal muscle tissue over other organs, such as the liver or kidneys, in this model. In fact, intact heart and skeletal muscle mitochondria from untreated and clofibrate-treated rats were capable of oxidizing C12.

Investigations of the chain-length dependency of DA β -oxidation showed, both *in vivo* and *in vitro*, medium oxidation for C12, with decreasing oxidizability for both

shorter and longer DAs.⁵⁵ The possible metabolic fates of DAs other than direct oxidation are gluconeogenesis and storage. This agrees with the data of Bergseth et al,⁵⁶ which showed that C12 is either oxidized or stored, inasmuch as only small amounts of it were found in the urine of rats given an intraperitoneal bolus, whereas approximately 28% to 39% of the radiocarbon administered as (1-12)¹⁴C-C₁₂ was excreted as ¹⁴CO₂.

There is *in vitro* and *in vivo* evidence that C12⁵⁶ can be esterified and incorporated into tissue lipids. In addition, many authors^{15,57-59} have suggested that even-numbered DAs are gluconeogenetic precursors *in vivo*. Osmundsen et al⁵⁹ showed that C12 is β -oxidized to succinate, and this represents the conclusive proof that net conversion of dicarboxylic fatty acids to glucose can take place in the animal. Kou et al¹⁸ also found that C12 is either directly converted into succinate or the β -oxidation of dodecanedioate results in acetyl-CoA being channeled into the tricarboxylic acid cycle. Therefore, C12 does not give rise to acetoacetate production; in fact, after administration of even-numbered dicarboxylic salts, the concentration of ketone bodies in blood decreases.⁵⁸

Our data confirm the above observations: not only is the urinary loss of C12 very small (3% to 5%), but also its tissue uptake is rapid (5% per minute, corresponding to a global half-life of about 13 minutes).

It is necessary to perform more detailed studies on DAs' long-term tolerance and their effects on protein metabolism. It will also be necessary to study administration forms different from disodium salts, which have a potential for sodium overloading and blood alkalization. Possible forms include DA triglycerides and DA amino acid derivatives. However, C12 might be a promising fuel substrate for use in parenteral nutrition because of the combination of several distinct characteristics. It delivers a sizable amount of energy per gram administered (7.181 kcal/g with a theoretical respiratory quotient of 0.77 upon complete oxidation); it is quickly cleared from plasma and metabolized; it does not induce ketone body formation⁵ but rather represents a good gluconeogenetic substrate¹⁸; and, by increasing the availability of Krebs cycle intermediates, it may favor the use of other conventional substrates as well.⁵⁸

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